



Nano-TiO₂ penetration of oral mucosa: *in vitro* analysis using 3D organotypic human buccal mucosa models

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BACKGROUND: Oral cavity is a doorway for a variety of products containing titanium dioxide (TiO₂) nanoparticles (NPs) (nano-TiO₂) such as food additives, oral healthcare products and dental materials. Their potential to penetrate and affect normal human oral mucosa is not yet determined.

OBJECTIVES: To evaluate the ability of nano-TiO₂ to penetrate the *in vitro* reconstructed normal human buccal mucosa (RNHBM).

METHODS: RNHBM was generated from primary normal human oral keratinocytes and fibroblasts isolated from buccal oral mucosa of healthy patients ($n = 6$). The reconstructed tissues were exposed after 10 days to clinically relevant concentrations of spherical or spindle rutile nano-TiO₂ in suspension for short (20 min) and longer time (24 h). Ultrahigh-resolution imaging (URI) microscopy (CytoViva™, Auburn, AL, USA) was used to assess the depth of penetration into reconstructed tissues. **RESULTS:** Ultrahigh-resolution imaging microscopy demonstrated the presence of nano-TiO₂ mostly in the epithelium of RNHBM at both 20 min and 24-h exposure, and this was shape and dose dependent at 24 h of exposure. The depth of penetration diminished in time at higher concentrations. The exposed epithelium showed increased desquamation but preserved thickness.

CONCLUSION: Nano-TiO₂ is able to penetrate RNHBM and to activate its barrier function in a dose- and time-dependent manner.

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Keywords: epithelium; nanoparticles; oral; organotypic model; titanium dioxide

Introduction

The unusual properties of nanomaterials (NMs) led to their use in, among others, oral hygiene products, food additives and dental materials (1–3). Their increased use raises concerns regarding the impact on biological systems (1, 2, 4).

Titanium dioxide (TiO₂) is one of the most used materials (5), due to its desirable properties. In bulk form, TiO₂ exhibits corrosion resistance, high biocompatibility, specific strength, low density, making it suitable for biomedical applications such as implants and vascular stents. At nano-level, the specific high surface area and the quantum effects lead to an increased chemical reactivity (1, 2). Titanium dioxide occurs mainly in three crystalline forms: anatase, rutile and brookite, each of them being associated with different properties and toxicological effects (5, 6). Increased use of nano-TiO₂ in paints, cosmetics, dental care products and food additives elevates the exposure risk via ingestion, inhalation and possible penetration through the oral mucosal tissues as well as skin. Oral mucosa is exposed to an array of NMs from various sources, oral intake of TiO₂ particles of 100–200 nm being reported to be considerably high (3). In UK, dietary consumption of TiO₂ has been estimated to be approx. 5 mg/person/day (3, 7). Although considered less hazardous than other NMs, nano-TiO₂ is non-degradable and can accumulate in different organs leading to chronic toxicity (2).

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Being several folds more permeable than skin, oral mucosa is an attractive site for drug delivery and toxicity studies (8). There are three types of oral mucosa: lining, masticatory and specialized tongue mucosa (9). Lining mucosa covers the mobile structures, is not keratinized, more elastic, deformable and more permeable as opposed to masticatory mucosa that lines gingivae and hard palate. In addition to its loosely packed nature, this makes lining mucosa more susceptible to penetration by external objects (10). Lining (buccal) mucosa has been subject to a considerable amount of research, mostly from a drug delivery/pharmaceutical point of view, but the penetration potential of nano-TiO₂ and possible related toxicological risks have been very little addressed. The aim of this study was to assess the penetration of nano-TiO₂ into human buccal mucosa by exposing *in vitro* 3D organotypic (OT) buccal mucosa models to two types of 40 nm rutile nano-TiO₂. The role of NM shape, that is spindle vs. spherical, was also evaluated.

Materials and methods

Nanoparticle characterization and preparation

Nano-TiO₂ is produced in a variety of shapes and sizes that are known to influence its interaction with cells (11). To study the role of NP shape, two types of rutile TiO₂ NMs were used in this study: spherical, 40 nm, (American Elements[®], Los Angeles, CA, USA) and spindle-shaped, 40 × 10 nm, (Nanostructured & Amorphous Materials Inc., Garland, TX, USA) (6), (Fig. 1). The particle concentrations were 5, 20 and 2000 mg/l, which are relevant for oral exposure to TiO₂ from various sources (7). Stock suspensions of 5 g/l nano-TiO₂ in deionized water were sonicated for 1 min with a 130-Watt ultrasonic processor at 70% duty (VCX130, Vibra-Cell, 130 W; Sonics & Materials Inc., Newtown, CT, USA) (12). Working suspensions were made by adding necessary volumes of culture medium immediately after sonication and rotated for at least 2 min. The NPs' shape and size in powder were previously characterized (6). The hydrodynamic diameter (HD), polydispersity index (PDI) and ζ-potential were measured using a Zetasizer Nano ZSP device (Malvern Instruments, Malvern, UK) both in stock solution and OT culture medium, the latter at time 0 and after 24 h.

Isolation of primary cells and generation of reconstructed normal human buccal mucosa (RNHBM)

Samples of human normal buccal mucosa were obtained during wisdom tooth extraction after informed consent ($n = 6$ healthy volunteers) and used for isolation of normal oral fibroblasts and keratinocytes. The biopsy was cleaned and washed twice with Dulbecco's modified Eagle's medium (DMEM) (Sigma, St Louis, MO, USA) supplemented with 2% antibiotics-antimycotics (Gibco, Grand Island, NY, USA) for 5 min. Tissue was then kept for 24 h in 20 mg dispase in 7.5 ml DMEM with 2% antibiotics-antimycotics at +4°C. The following day epithelium was easily and completely separated from connective tissue with the help of tweezers. Fibroblasts were isolated from connective tissue explants and cultured in DMEM with 10% foetal bovine

serum (FBS) and 1% antibiotics-antimycotics. Keratinocytes were obtained by trypsinization of epithelium (10× Trypsin-EDTA) (Sigma) and cultured in keratinocyte serum-free medium (KSFM) supplemented with 1 ng/ml human recombinant epidermal growth factor, 25 µg/ml bovine pituitary extract (Gibco) and 1% antibiotics-antimycotics. Both cell types were propagated and expanded in their specific culture medium for 2–4 passages (13). From each biopsy, a set of organotypic tissues was constructed from keratinocytes and fibroblasts from the same donor.

Exposure of RNHBM to nano-TiO₂, tissue harvesting and processing

In order to avoid the leakage and to prevent exposing of organotypic tissue from the bottom (connective tissue part), a drop of only 20 µl of nano-TiO₂ suspended in medium was placed on the top of the model, precisely in the middle. Tissues in which the suspension poured over *t* edges were excluded from the analysis. Tissues were harvested within 20 min and after 24 h of exposure, washed in phosphate-buffered saline (PBS) (Gibco) thrice and fixed with 10% buffered formalin for 24–48 h. RNHBM tissues were processed separately for each type of NPs and exposure time. Tissues were washed once in PBS, twice in distilled water, dehydrated in graded ethanol baths and then kept 30 min in xylene, followed by paraffin baths (Paraplast X-TRA[®]). Histological sections (3 µm thickness) were cut with a sliding microtome (Leica SM2000R, Leica Biosystems Nussloch GmbH, Heidelberg, Germany), placed on glass slides cleaned with ethanol and then stained with Haematoxylin-Eosin in a Tissue-Tek[®] Prisma[™] slide steiner (Sakura Seiki Co., Ltd, Nagano, Japan).

Ultrahigh-resolution microscopy and image analysis

Ultrahigh-resolution imaging (URI) (CytoViva[™], Auburn, AL, USA) was employed to assess penetration of nano-TiO₂ into RNHBM using a 100× oil immersion objective. CytoViva[™] is a high contrast optical dark-field system with an annular condenser; light is collimated without loss of intensity at oblique angles giving improved contrast and signal-to-noise ratio (90 nm resolution) (14). Nanoparticles and other light scattering objects appear as bright features on a dark background (15); therefore, the fluorescent marking of NPs, which might modify their physicochemical properties, is not needed. The average tissue length was approximately 10 mm. To reduce bias and obtain representative information from the tissues, when taking pictures, the peripheral parts (0.2 mm) of tissues were excluded and images were taken at a 1-mm interval. A qualitative screening of the reconstructed mucosa of the OTs was performed before starting the measurements and the tissues without epithelium, with discontinuous epithelium, or with an epithelium less than 20 µm thickness, were excluded from the analysis. Image analysis was performed with NIS-Elements software (v. 2.3, Nikon, Japan).

Statistical analysis

Data were expressed as mean ± standard error of the mean (SEM). A general linear model was used to compare means

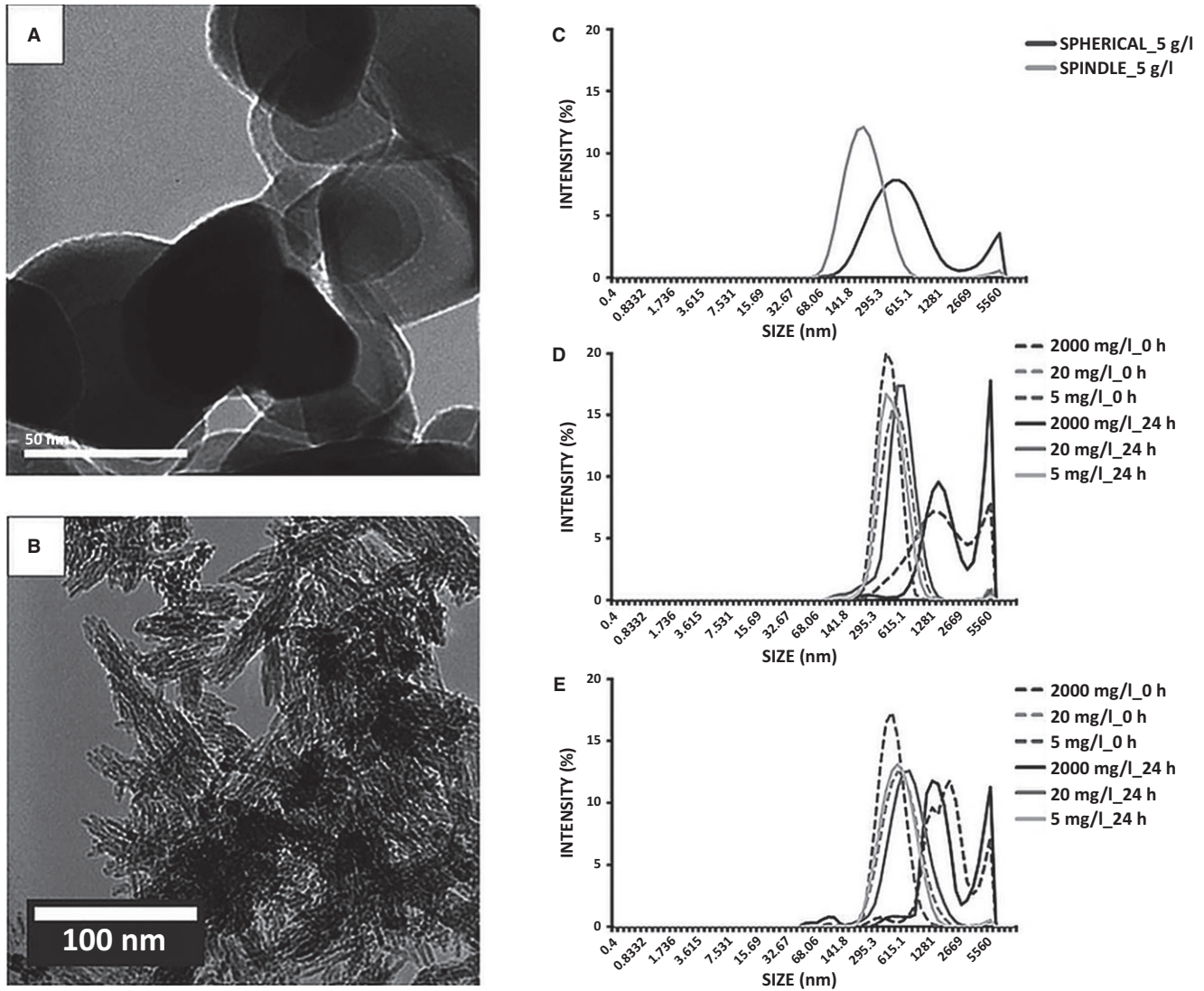


Figure 1 TEM images of the nano-TiO₂ powders: spherical nano-TiO₂ (A) and spindle nano-TiO₂ (B). Hydrodynamic size distribution as shown by the DLS measurements: batch suspension in distilled water for both types of particles (C), spherical nano-TiO₂ in FAD-OT medium exposure media (time 0 and 24 h) (D) and spindle-shaped nano-TiO₂ in FAD-OT medium exposure media (time 0 and 24 h) (E).

within and between different treatment groups. A *P*-value of <0.05 was considered statistically significant.

Ethical considerations

A written informed consent was retrieved from each patient prior to the start of the study. The study was approved by Regional Committee for Medical and Health Research for Western Norway (2013/1492/REK Vest).

Results

Spindle-shaped nano-TiO₂ formed smaller agglomerates and were more stable in suspension

The shape of nano-TiO₂ particles was confirmed by TEM (Fig. 1A,B, Table 1) as previously reported (6). Spherical nano-TiO₂ formed larger agglomerates in ^{dd}H₂O (459.93 ± 18.36 nm) compared to spindle-shaped agglomerates (180.67 ± 2.25) (Fig. 1C, Table 1). In the medium, spherical particles also formed larger agglomerates, except

at 2000 mg/l. Agglomerate sizes increased with time, larger agglomerates being registered after 24 h (Fig. 1D,E, Table 1). The ζ-potential in ^{dd}H₂O revealed a higher absolute value for the spindle-shaped particles, indicating their higher stability in suspension, a result that correlates well with their smaller agglomerates' sizes. Nevertheless, the ζ-potentials were relatively similar at all concentrations and over time in culture medium (Table 1).

Spindle-shaped nano-TiO₂ was found more superficially than spherical ones in the epithelium of RNHBM

All reconstituted tissues displayed a well-differentiated stratified squamous epithelium with a distinct basal, spinous and superficial non-keratinized cell layer, on top of a connective tissue equivalent, similar to native human buccal mucosa (Fig. 2A). Nano-TiO₂ agglomerates were visualized as bright white/bluish objects by URI due to their high refractive index (Fig. 3B,C) and were observed both over

Table 1 Physicochemical characteristics of nano-TiO₂ in powder form, water and culture medium

		Spherical Nano-TiO ₂ (Ti2)			Spindle Nano-TiO ₂ (Ti4)			
Supplier's description		Rutile 40 nm (TI-OX-02-NP.050; American Elements [®] , USA)			Rutile 40 × 10 nm (#5480MR; Nanostructured & Amorphous Materials Inc., USA)			
S _{BET} (m ² /g) ^a		38			165			
D _{BET} (nm) ^b		37			Not spherical			
Crystal structure		92% Rutile 8% Anatase			100% Rutile			
Crystal size (nm) ^c		Rutile: 21			Rutile: 8.5			
IEP ^d		–			3.10			
Circularity ± SD ^e		0.79 ± 0.08			0.29 ± 0.04			
MECD ± SD ^f		36 ± 22			14 ± 6			
		H.d. ^g	Pdi ^h	zeta ⁱ	H.d.	Pdi	zeta	
Batch (in MiliQ water)	5 g/l	459.93 ± 18.36	0.41 ± 0.04	0.30 ± 1.10	180.67 ± 2.25	0.21 ± 0.01	–26.52 ± 0.80	
In FAD-OT medium	5 µg/ml	0 h	469.12 ± 30.62	0.45 ± 0.05	–8.55 ± 0.57	401.54 ± 9.50	0.38 ± 0.06	–9.70 ± 0.89
		24 h	545.01 ± 62.63	0.53 ± 0.04	–9.03 ± 0.65	404.65 ± 13.31	0.35 ± 0.04	–9.44 ± 0.80
	20 µg/ml	0 h	514.94 ± 24.31	0.31 ± 0.05	–8.83 ± 1.30	468.99 ± 7.23	0.26 ± 0.02	–9.45 ± 1.09
		24 h	671.58 ± 65.56	0.53 ± 0.07	–10.8 ± 0.8	571.10 ± 9.11	0.28 ± 0.03	–9.75 ± 0.55
	2000 µg/ml	0 h	1105.47 ± 183.29	0.38 ± 0.04	–9.11 ± 2.86	2389.35 ± 503.66	0.63 ± 0.21	–12.04 ± 0.99
		24 h	2079.12 ± 393.21	0.43 ± 0.08	–10.65 ± 1.54	3398.20 ± 460.93	0.51 ± 0.12	–12.60 ± 0.79

^aSpecific surface area.

^bCalculated particle's diameter from BET measurements, DBET = k/q_{SBET} , $k = 6$ for a sphere. q is the density of the powder.

^cCalculated using Scherrer equation: $D = kk/b_{\cosh}$. A. (anatase, 101), R. (rutile, 110).

^dIsoelectric point from titration curve: zeta potential vs. pH in aqueous solution of 0.14 M NaCl.

^eCircularity from TEM pictures of NPs (from 0 to 1, where 1 is a perfect circle).

^fAverage microscopy equivalent circle diameter (nm) from TEM pictures of NPs.

^gHydrodynamic diameter.

^hPolydispersion index.

ⁱZeta potential.

The physicochemical characteristics in powder form were reproduced from Allouni et al. (6), with permission.

and within the epithelium. Larger agglomerates were seen over the epithelial layer at higher NP concentrations. At the highest concentration, an almost continuous bright belt of NP agglomerates covered the epithelium (Fig. 3B,C). Both types of nano-TiO₂ were identified by URI within RNHBM epithelium at early (20 min) as well as late (24 h) time points. Generally, spherical NPs were found deeper in the epithelium compared to spindle-shaped ($P = 0.034$) (Fig. 4), although the difference was statistically significant only for the highest concentration at the early time of exposure ($P = 0.031$).

Penetration of nano-TiO₂ was dose-dependent only at later (24 h) but not at early (20 min) time point

The location of NPs within epithelium was similar for both types and all concentrations at the early time point (20 min) ($P > 0.05$) (Fig. 4). After 24 h, concentration-dependent differences were observed. Thus, spherical nano-TiO₂ showed the deepest location at 5 mg/l concentration, and this was significantly deeper than at 20 and 2000 mg/l ($P = 0.006$ and $P = 0.023$, respectively). The same trend was observed for spindle-shaped NPs, although the difference was not statistically significant.

Penetration of nano-TiO₂ was time dependent at high concentrations (20 and 2000 mg/l) only

The level of epithelium penetration did not change with exposure time at the lowest concentration, regardless of NP shape. A significant decrease in the penetration depth was observed at 24 h at higher concentrations (Fig. 5) for both

types of particles ($P = 0.04$). The difference was statistically significant for spherical NPs at 2000 mg/l ($P = 0.001$) and spindle-shaped at 20 mg/l ($P = 0.022$).

Tissues exposed to nano-TiO₂ showed increased desquamation but preserved epithelial thickness

Tissue architecture and microanatomy was not altered by exposure to nano-TiO₂ (Figs 2 and 3). At higher concentrations, increased desquamation of the superficial epithelial layers was observed, especially for tissues exposed to spherical nano-TiO₂ (Figs 2 and 3). Epithelial thickness of RNHBM tissues was either constant or increased after 24 h of exposure to both types of nano-TiO₂, although the change was not statistically significant (Fig. 5).

Discussion

To our knowledge, this is the first study that assessed the penetration of nano-TiO₂ into a human buccal mucosa 3D organotypic model. Employment of a 3D model has the advantage of reconstructing in a standardized and reproducible manner the architecture of original tissue, allowing thus cell-to-cell and cell-to-matrix interactions and bringing the experimental context as close as possible to the *in vivo* settings. Nevertheless, although superior to monolayer experimental systems, the 3D organotypic model used in this study lacks vascular and immunocompetent compartments that play an important role in epithelial barrier functions (16). Moreover, *in vivo*, the epithelium of oral cavity is moistened with saliva, known to have protective

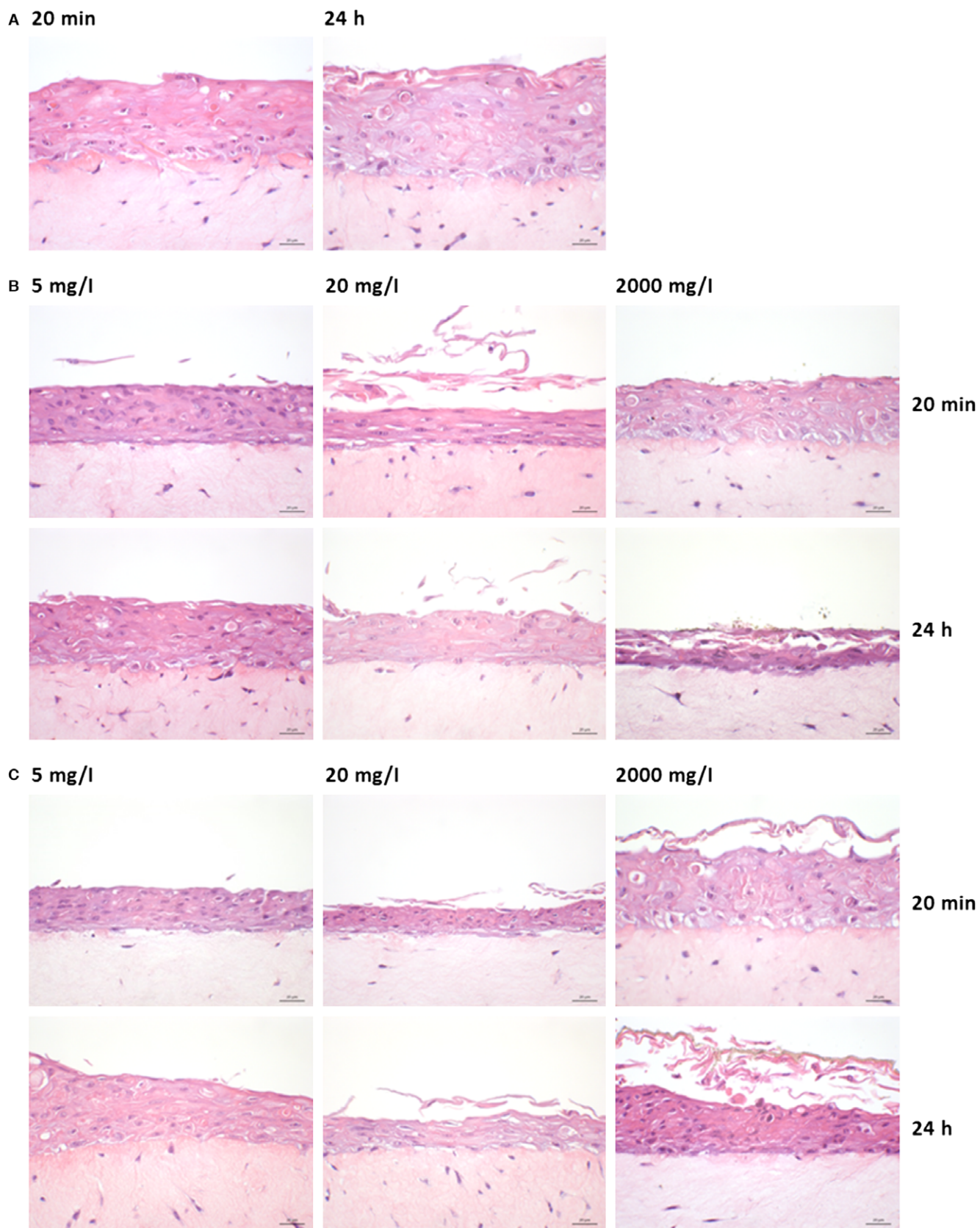


Figure 2 Representative light microscopy images of unexposed (A) and nano-TiO₂ exposed (B, C) 3D organotypic tissues for 20 min and 24 h. The reconstructed normal human oral buccal tissues were harvested, fixed in formalin, embedded in paraffin, sectioned and haematoxylin–eosin stained. Control (A), spherical nano-TiO₂ (B), spindle nano-TiO₂ (C). Scale-bar: 20 μm.

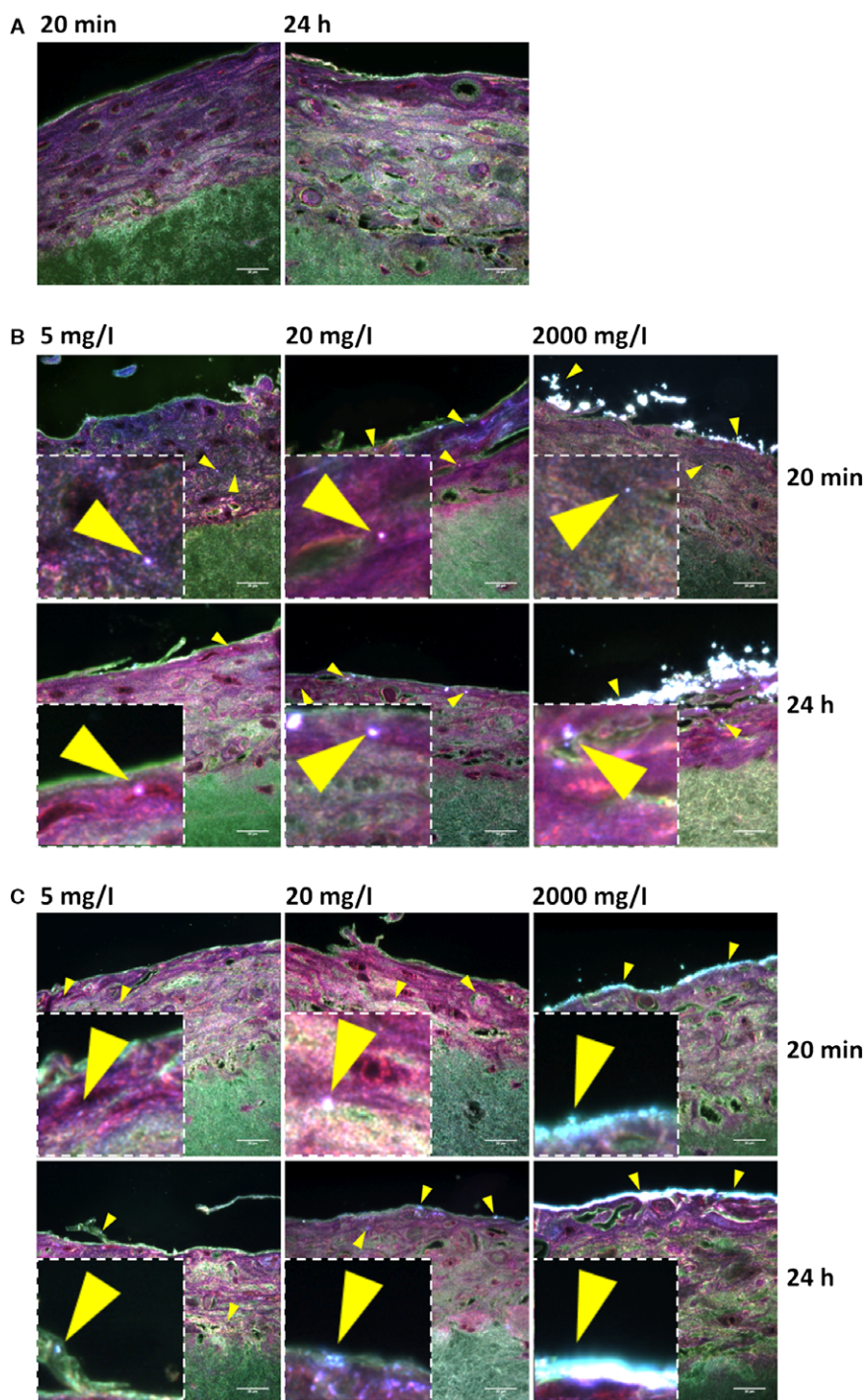


Figure 3 Representative URI (CytoViva) images of unexposed (A) and nano-TiO₂ exposed (B, C) 3D organotypic tissues for 20 min and 24 h. The reconstructed normal human oral buccal tissues were harvested, fixed in formalin, embedded in paraffin, sectioned and haematoxylin–eosin stained before URI microscopy. Nanoparticle agglomerates were identified as white/blue bright spots as indicated by arrow heads. Control (A), spherical nano-TiO₂ (B), spindle nano-TiO₂ (C). Scale-bar: 20 μm. Inserts show zoom out of the regions of interest, where white/blue bright spots were mainly present.

properties and contain mucus that has an impact on the mobility of NPs. Thus, the 3D organotypic model used here might have been more susceptible to penetration by nano-TiO₂ and might have undergone more severe modifications after exposure than native tissues. However, recent studies have shown that smaller NPs, *that is* around 20 nm, in contrast to 200 nm, are able to penetrate through the layer of

mucins precipitated on the surface of oral epithelium *in vivo* (17). This indicates that for smaller NPs, the effects seen *in vitro* on the OTs may actually be representative for the *in vivo* effects.

The DLS measurements showed relatively large agglomerate sizes, especially for spherical nano-TiO₂, which increased with concentration. The NP ζ-potential may

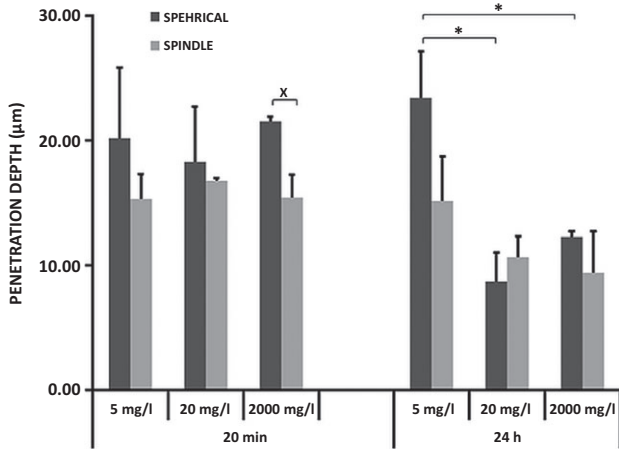


Figure 4 Location (penetration depth) of spherical- and spindle-shaped nano-TiO₂ into the epithelium of RNHBM after 20 min and 24 h of exposure. Statistical significant difference in the depth of penetration between the different concentrations of spherical nano-TiO₂ is marked by stars (*). Statistical significant difference in the depth of penetration between the two shapes of nano-TiO₂ is marked by cross (x).

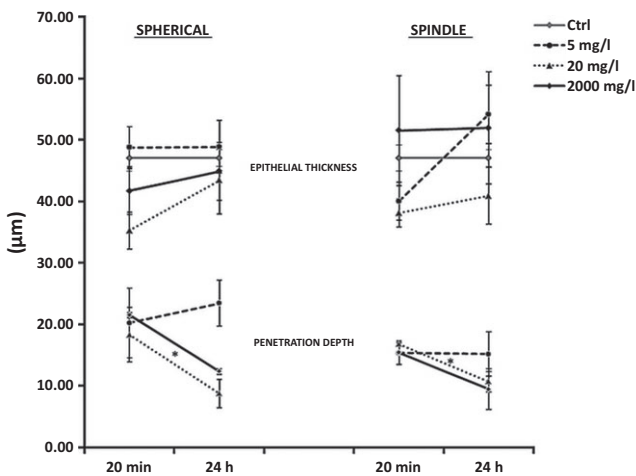


Figure 5 Time-dependent variations of penetration depth of nano-TiO₂ particles and epithelial thickness of RNHBM exposed to nano-TiO₂. Statistical significant difference in the depth of penetration with time is marked by stars (*).

explain the agglomeration degree, as spherical particles had significantly lower ζ -potential values compared to the spindle-shaped (Table 1). However, smaller agglomerates of nano-TiO₂ might be present in suspensions although not detected via DLS (18), which may explain why we could detect NPs as deep as one-third within the epithelium at all concentrations for both NP types.

Although smaller agglomerates were associated with spindle-shaped particles, they were located more superficially in the epithelium compared to the spherical. Similar findings were obtained by other research groups who reported that spindle-shaped particles were taken up less by cells as compared to the spherical of the same crystal structure (6, 19). The lower uptake of spindle-shaped particles has been suggested to be associated with their

high aspect ratio, as it takes longer time for a cell membrane to wrap around the elongated particles (20). It has been well established that the shape plays an important role in the nano-TiO₂ agglomeration in biological media (12), as well as on the tissue and cellular response (11, 21).

The URI analysis revealed that both nano-TiO₂ types, regardless of concentration, were located approximately at the same level within epithelium after 20 min of exposure (Fig. 4). After 24 h, tissues exposed to 5 mg/l displayed NPs located deeper compared to those of 20 and 2000 mg/l. It has been shown that the concentration has significant influence on the rate of agglomeration, which increases over time in suspensions with high concentrations (12). As known, larger agglomerates have less potential to penetrate the epithelial barrier (17). Nevertheless, as indicated by our results, another important factor contributing to the more superficial location observed at higher concentrations with time might be the desquamative response of the tissues as RNHBM is not passive membranes, but biologically active systems. Unfortunately, the degree of desquamation could not be quantified, but its presence was clearly associated with exposure to nano-TiO₂, especially at higher concentrations. Desquamation is one of the most efficient modalities through which stratified squamous epithelia of the body, including buccal mucosa, eliminate potentially harmful agents (22). Similar to native buccal epithelium, RNHBM has a stratified epithelium that maintains its homeostasis by the balance between basal cell proliferation and cell loss at the surface (desquamation) (13). The fact that epithelial thickness remained the same over time after exposure despite increased cell loss (desquamation) indicates an increase in basal cell proliferation of exposed RNHBM to compensate this cell loss. These findings suggest that release of inflammatory cytokines and chemokines via MAP Kinase and NF- κ B signalling cascades might be a possible outcome of the cellular exposure to nano-TiO₂, leading to the increased epithelial tissue proliferation observed in this work (23, 24). Nonetheless, these findings do not exclude that proliferation might as well have been a compensatory epithelial tissue reaction due to a direct effect on the genetic components of the cells, as previous reports showed that nano-TiO₂ is able to induce DNA strand breaks and genetic instability (24). This increased reactive proliferation is part of the physiological barrier function, but due to wide use of nano-TiO₂ in a variety of products, one might expect that repeated exposures may either exhaust the proliferative capacity of epithelium, finally resulting in epithelial atrophy, or will lead to cell transformation and malignancy due to accumulation of replication errors as a consequence of a prolonged increased proliferation (25).

The permeability and the barrier function of stratified epithelial tissues have been long attributed mainly to superficial layers of the tissue (26). Thus, once a foreign object goes through the top layer of epithelium (crosses the intercellular lipids secreted by the membrane-coating granules on the superficial layers), it is highly likely that this object would reach the underlying connective tissues (8). In the present study, both types of nano-TiO₂ particles crossed the superficial epithelial layers regardless of exposure time

and concentration, indicating that in general, particles are able to penetrate the oral epithelial barrier in a relatively short time if they are at the right size. Nevertheless, nano-TiO₂ particles located in the connective tissue equivalents were found quite rare at any concentration or time point, and together with the finding that the NPs were found even more superficially after 24 h, on the way to be eliminated from the epithelium, dismisses the theory of Caon et al. (8). However, the presence of particles at deeper levels at lower concentrations suggests that due to a lower degree of agglomeration, low doses may be actually more toxic, as also indicated by previous *in vitro* studies (27).

Objects penetrate epithelial barriers by one of two routes: trans-cellular and para-cellular (8). Uptake of nano-TiO₂ by buccal epithelial cells was reported to take place as soon as 10 min after exposure, their internalization via endocytosis and then trans-cellular transport enabling them to travel fast and deeper into the tissues (28, 29). Microplacae were reported to play an important role in NPs/agglomerates internalization into epithelial tissues in a size-dependent manner meaning that objects need to be small enough to fit in the furrows (200–400 nm) (28, 30). Although we did not investigate the route of transport within epithelium, the location of nano-TiO₂ below the upper third of epithelium within 20 min after exposure suggested a para-cellular way of transport, as it would have taken much longer for the NPs to reach this far down via a trans-cellular route alone.

Conclusion

In summary, nano-TiO₂ penetrated a reconstituted human normal buccal epithelium very soon after exposure. The penetration was shape-, dose- and time-dependent, and most of the particles remained within the upper third of the epithelial tissue. Maintained epithelial thickness despite increased desquamation at higher concentrations and longer exposure time indicates that nano-TiO₂ particles induced a biological response in the epithelium. Although within physiological limits after single exposures, these effects might trigger changes with adverse consequences in the long term, indicating the need for further characterization of the effects of nano-TiO₂ exposure.

References

1. Nel A, Xia T, Mädler L, et al. Toxic potential of materials at the nanolevel. *Science* 2006; **311**: 622–7.
2. Oberdörster G, Oberdörster E, Oberdörster J. Nanotoxicology: an emerging discipline evolving from studies of ultrafine particles. *Environ Health Perspect* 2005; **113**: 823–39.
3. Powell JJ, Faria N, Thomas-Mckay E, et al. Origin and fate of dietary nanoparticles and microparticles in the gastrointestinal tract. *J Autoimmun* 2010; **34**: J226–33.
4. Donaldson K, Stone V, Tran C, et al. Nanotoxicology. *Occup Environ Med* 2004; **61**: 727–8.
5. Weir A, Westerhoff P, Fabricius L, et al. Titanium dioxide nanoparticles in food and personal care products. *Environ Sci Technol* 2012; **46**: 2242–50.
6. Allouni ZE, Høl PJ, Cauqui MA, et al. Role of physicochemical characteristics in the uptake of TiO₂ nanoparticles by fibroblasts. *Toxicol In Vitro* 2012; **26**: 469–79.
7. Jovanović B. Critical review of public health regulations of titanium dioxide, a human food additive. *Integr Environ Assess Manag* 2015; **11**: 10–20.
8. Caon T, Jin L, Simões CO, et al. Enhancing the buccal mucosal delivery of peptide and protein therapeutics. *Pharm Res* 2015; **32**: 1–21.
9. Garant PR, Garant P. *Oral cells and tissues*. Hanover Park, IL: Quintessence Publishing Company, 2003.
10. Harris D, Robinson JR. Drug delivery via the mucous membranes of the oral cavity. *J Pharm Sci* 1992; **81**: 1–10.
11. Duan X, Li Y. Physicochemical characteristics of nanoparticles affect circulation, biodistribution, cellular internalization, and trafficking. *Small* 2013; **9**: 1521–32.
12. Allouni ZE, Cimpan MR, Høl PJ, et al. Agglomeration and sedimentation of TiO₂ nanoparticles in cell culture medium. *Colloids Surf B* 2009; **68**: 83–7.
13. Costea DE, Loro LL, Dimba EAO, et al. Crucial effects of fibroblasts and keratinocyte growth factor on morphogenesis of reconstituted human oral epithelium. *J Invest Dermatol* 2003; **121**: 1479–86.
14. Luque-Garcia JL, Sanchez-Díaz R, Lopez-Heras I, et al. Bioanalytical strategies for in-vitro and in-vivo evaluation of the toxicity induced by metallic nanoparticles. *Trends Analyt Chem* 2013; **43**: 254–68.
15. Vainrub A, Pustovyy O, Vodyanov V. Resolution of 90 nm ($\lambda/5$) in an optical transmission microscope with an annular condenser. *Opt Lett* 2006; **31**: 2855–7.
16. Costea DE. Epithelial-mesenchymal interactions in normal and neoplastic human oral mucosa. A study on in vitro organotypic models. PhD thesis, Alkopi, UiB, Norway ISBN 82-8006-022-70. 2005.
17. Roblegg E, Fröhlich E, Meindl C, et al. Evaluation of a physiological in vitro system to study the transport of nanoparticles through the buccal mucosa. *Nanotoxicology* 2012; **6**: 399–413.
18. Ramirez-Garcia S, Chen L, Morris MA, et al. A new methodology for studying nanoparticle interactions in biological systems: dispersing titania in biocompatible media using chemical stabilisers. *Nanoscale* 2011; **3**: 4617–24.
19. Chen J, Zhou H, Santulli AC, et al. Evaluating cytotoxicity and cellular uptake from the presence of variously processed TiO₂ nanostructured morphologies. *Chem Res Toxicol* 2010; **23**: 871–9.
20. Verma A, Stellacci F. Effect of surface properties on nanoparticle–cell interactions. *Small* 2010; **6**: 12–21.
21. Fubini B, Ghiazza M, Fenoglio I. Physico-chemical features of engineered nanoparticles relevant to their toxicity. *Nanotoxicology* 2010; **4**: 347–63.
22. Senel S, Kremer M, Katalin N, et al. Delivery of bioactive peptides and proteins across oral (buccal) mucosa. *Curr Pharm Biotechnol* 2001; **2**: 175–86.
23. Chen H-W, Su S-F, Chien C-T, et al. Titanium dioxide nanoparticles induce emphysema-like lung injury in mice. *FASEB J* 2006; **20**: 2393–5.
24. Trouiller B, Reliene R, Westbrock A, et al. Titanium dioxide nanoparticles induce DNA damage and genetic instability in vivo in mice. *Cancer Res* 2009; **69**: 8784–9.
25. Preston BD, Albertson TM, Herr AJ. DNA replication fidelity and cancer. *Semin Cancer Biol* 2010; **20**: 281–93.
26. Squier C. The permeability of oral mucosa. *Crit Rev Oral Biol Med* 1991; **2**: 13–32.
27. Vamanu CI, Cimpan MR, Høl PJ, et al. Induction of cell death by TiO₂ nanoparticles: studies on a human monoblastoid cell line. *Toxicol In Vitro* 2008; **22**: 1689–96.
28. Teubl BJ, Leitinger G, Schneider M, et al. The buccal mucosa as a route for TiO₂ nanoparticle uptake. *Nanotoxicology* 2014; **9**: 1–9.

29. Schoelermann J, Burtey A, Allouni ZE, et al. Contact-dependent transfer of TiO₂ nanoparticles between mammalian cells. *Nanotoxicology* 2015; **10**: 1–12.
30. Teubl BJ, Meindl C, Eitzlmayr A, et al. In-vitro permeability of neutral polystyrene particles via buccal mucosa. *Small* 2013; **9**: 457–66.

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Conflict of interest statement

None to declare.